

CT Registry Re	view
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May 19, 2018 and May 20, 2018

CT Physics

May 20, 2018

Content Specs:			
Patient Care			
• 22 • Safety			
• 20			
Image Production55			
Procedures68			
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Content Specs:		-	
Patient Care			
• 22			
• Safety Image Formation – 30 • 20			
Image Production			
• 55 • Procedures Image Evaluation and Archiving - 25			
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	Losri		
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Objectives			
• Identify the basic components, as well as their functions, of a CT sci	anner.		
 Define CT Scanner geometry as it relates to detector configuration. Explain the CT imaging parameters and their relationship to the phyprinciples of radiation interaction. 	/sical		
principles of radiation interaction.Discuss the different methods of image acquisition and reconstruct			
 Explain the principles of image quality and how image display effect principles. 			
 Discuss artifacts; their causes and how to resolve them. 			
 Define and explain the post-processing techniques used in CT. Discuss the archiving, networking and security of CT images. 	osrt		
	One became a Australia Communication		

Image F	ormation
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- CT System Principles, Operation, and Components
- Imaging Parameters and Data Acquisition
- Imaging Processing



Image Formation

- CT System Principles, Operation, and Components

 - 1. Tube
 X-ray production
 Warm-up procedures
 2. Collimation/beam width
 - 3. Generator
- 4. Detectors
 Detector configuration
 Detector collimation
 S. Data Acquisition
 Computer and Array Processor



Image Formation:

CT System Principles, Operation, and Components

- The CT Scanner System
 - The CT x-ray tube generator
 - The CT x-ray tube
 - The CT beam filter
 - The CT collimators
 - \bullet The CT detectors and the DAS
 - The computer



Image Formation:	
CT System Principles, Operation, and Components	
Generator CT scanners use three-phase power	-
High frequency generators	
 Located within the CT gantry Low-voltage, low frequency AC current is changed to high-frequency 	
DC current for use by the CT x-ray tube • Power ratings range from 20 to 100kW	
<u> </u>	
© 2018 OSAT_Gial Dozels 10	
Image Formation: CT System Principles, Operation, and Components	
• Tube	
Rotating anode CT x-ray tubes made of rhenium, tungsten, and molybdenum (RTM) alloy	
 CT x-ray tubes for spiral imaging may include a graphite base body for high thermal capacity Small target angle (12 degrees) 	-
Rotation speed of 3600 to 10,000 revolutions per minute Straton CT X-ray tube	
Useful for MSCT scanners Anode is immersed in oil, resulting in high cooling rates	
 Allows for high mA and long exposure times for increasing anatomical coverage Cathode consists of an electron beam that is deflected to strike the anode 	
at two focal spots.	

Image Formation:

CT System Principles, Operation, and Components

- Tube

 X-ray production
 Bremsstrahlung "brems" breaking or slowing (German origin)
 Incident electron and the nucleus
 Characteristic
 Incident electron and inner shell electron
 Reactions
 Incident electron and inner shell electron
 Characteristic
 Incident electron and inner shell electron

 A characteristic
 Incident electron and inner shell electron

 A characteristic
 Incident electron
 Inc



Image Formation: CT System Principles, Operation, and Components	
• Tube	
Warm-up procedures Diagnostic imaging systems need a warm-up period before the system performs optimally. This may include the boot-up of the system and	
operating system, warm-up of the x-ray tube, calibration of detectors, and stabilization of displays.	
In CT, an air calibration is usually carried out at least on a daily basis. Certain manufacturers also build an x-ray tube warm-up procedure into the boot-up of the system, which has to be completed before the	
system will function.	
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Image Formation: CT System Principles, Operation, and Components	
CT x-ray tube filtration	
Removes long wavelength x-rays(low and slow) that do not play a role in CT image formation.	
Produces a "harder" beam Reduces patient dose	
Shapes the energy distribution across the radiation beam to produce uniform beam hardening	
umom beam natueming	
OCH.	
(USI I)	-
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Image Formation:	
CT System Principles, Operation, and Components	

• Collimation/beam width

Prepatient Postpatient Predetector

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Image Formation:	
CT System Principles, Operation, and Components	
Formation of CT Images	
The formation of CT images by a CT scanner involves 3 steps	
Data acquisition	
Image reconstruction Image display	
Manipulation	
Storage Networking	
<u>nsrt</u> l	
(O)IE	
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Image Formation:	
CT System Principles, Operation, and Components	
Data Acquisition System – DAS	
 Refers to the collection of x-ray transmission measurements from the patient Special electronic detectors measure the attenuation of the x-ray beam as it 	
passes through the patient. • Geometry	
 The construction arrangement of the CT x-ray tube and the detectors used in the collection of transmission measurements. 	
Historically: 1 st generation – Pencil beam	
2 nd generation – Fan beam 3 nd generation – Spiral – Fan beam	
4 th generation – Fixed detector – Spiral – Fan beam 5 th generation – EBCT 6 th generation – Dual source - Spiral – Fan beam	
7th generation – Flat panel DR or detector bank – Cone beam	-
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Image Formation:	
CT System Principles, Operation, and Components	
Detectors	
• Types of detectors	
Energy Integration detector (EI) Dual Layer detector	
Dual Layer detector Direct Conversion detector	
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Image Formation: CT System Principles, Operation, and Components
Detectors Convert x-ray photons to electrical energy. Electrical energy then becomes digital data. Detector materials: Solintillation Detector Solid state detectors that consist of a scintillation crystal coupled to a photodiode. Used to improve the performance efficiency of the detector to improve image quality and reduce artifacts. Scintillation crystal converts the x-ray photons into light photons. The photodiode converts the light photons into electrical signals.
osrt

Image Formation:

CT System Principles, Operation, and Components

- - Scintillation Crystals used in CT
 - Cadmium tungstate and a ceramic material
 - Rare Earth Oxides
 - Yttria
 - Gadolinium Oxysulfide (UFC)
 - Ultrafast ceramic (UFC)
 - Most recently Lutetium (Lu) based garnet has been introduced for use in CT.



Image Formation:

CT System Principles, Operation, and Components

- Detectors Dual layer
 - Scintillation Crystal
 - Top layer low density scintillator Zinc Selenide (ZnSe)
 - Absorbs low energy x-ray photons
 Bottom layer high density scintillator (gadolinium oxysulfide)
 - Absorbs high energy x-ray photons
 - Both are a scintillation crystal coupled to a photodiode.
 - Both layers are integrated to ensure optimum performance.



Image Formation:	
CT System Principles, Operation, and Components	
• Detectors	
Proprieties of detectors Capture efficiency	
Absorption efficiency	
• Stability	
Response time	
Afterglow Dynamic range	
Dynamic range	
nort	
0316	
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Image Formation:	
CT System Principles, Operation, and Components	
• Detectors	
Detectors Detector configuration	
 Describes the number of data collection channels and the effective 	
section thickness determined by the data acquisition system settings.	
	-
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OSTU	
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Image Formation:	
CT System Principles, Operation, and Components	
• Detectors	
1. measures the transmitted radiation beam Based on attenuation properties	
Encodes these measurements into binary data	
3. Transmits binary data to the computer	
Where they will be assigned CT numbers	
OCT	
USI (
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		-
Image Formation:		
CT System Principles, Operation, and Components		
 Attenuation – CT Numbers – aka Hounsfield numbers Window Width – Image Contrast Window Level – Image Brightness 		
- window level – image brightness		
	nerl	
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		1
Image Formation: CT System Principles, Operation, and Components		
Computer and Array Processor		
High speed Large amount of storage		
• Fast		
	<u>ocrl</u>	
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		1
Image Formation:		
CT System Principles, Operation, and Components • Patient table		
Operators Console		
	ocri.	
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Image Formation - CT System Principles, Operation, and Components		
 Imaging Parameters and Data Acquisition 1. Parameters 		
• kVp		
• mAs		
PitchAcquisition thickness		
• x,y,z planes		
Scan field of view		
2. AcquisitionAxial/sequential		
Helical/spiral	D-1.	
Volumetric	osrt	
Imaging Processing © 2018 OSRT_Glatousis		
e 2018 OSKI, Pallonitis	28	
Image Formation:		
Imaging Parameters and Data Acquisition		
• 1. Parameters		
• kVp		
• mAs		
• Pitch		
 Acquisition thickness 		
• x,y,z planes		
 Scan field of view 		
	OCT	
	[กิวเเ	
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Image Formation:		
Imaging Parameters and Data Acquisition		
• kVp		
 Typical kVp settings: 100, 120, 140 		
 Used to adjust the energy level of the x-ray beam 		
 Controls the contrast of the image 		
	osrt	
	[USI t	

Image Formation: Imaging Parameters and Data Acquisition	
• mAs	
mA and Scan Time mA controls the quantity of x-rays	
CT mAs settings are relatively high (200 mAs) Increased scan time increases the x-ray photons	
ner	
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Image Formation: Imaging Parameters and Data Acquisition	
• Pitch	
 The ratio of the distance the table travels per revolution (in millimeters) to the total nominal beam collimation (in millimeters). 	
Toort	
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Image Formation: Imaging Parameters and Data Acquisition	
Acquisition thickness	
How much of the anatomy will be covered or acquired.	
ner!	
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	<u> </u>

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Image Formation: Imaging Parameters and Data Acquisition	
 x,y,z planes Z plane = axial plane – The CT main plane 	
 X plane is a Sagittal plane (a reconstruction plane) Y plane is a Coronal plane (a reconstruction plane)	
F=-1.4-	
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	_
Image Formation:	
Imaging Parameters and Data Acquisition	
 Scan field of view Area of anatomy to scan in centimeters (cm) 	
 Display field of view Area of scanned anatomy to be displayed on the monitor. Further discussed in the next section! 	
diseased in the next section:	
F24.	
© 2014 COSTT Galocosts	
© 2018 OSRT_Gialousis 35	·
Image Formation:	
Imaging Parameters and Data Acquisition • 2. Acquisition	
Axial/sequential Helical/spiral	
Volumetric	
54.	
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Image Formation:	
Imaging Parameters and Data Acquisition	
Axial/sequential (Slice by Slice)	
The CT x-ray tube rotates around the patient.	
The CT x-ray tube rotates around the patient. The CT x-ray tube stops and the patient is moved, via the CT table,	
into the next defined scan position.	
 Process continues until the entire region of interest is scanned. 	
USIT	-
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Image Formation:	
Imaging Parameters and Data Acquisition	
Helical/spiral	
 Continuous rotation of the CT x-ray tube around the patient. 	
 Made possible by the slip ring. 	
Patient is moved through the gantry aperture as the CT x-ray tube	
rotates around the patient's body.	
 Process continues until the entire region of interest is scanned. 	
COCH	
<u> </u>	
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Image Formation:	
Imaging Parameters and Data Acquisition	
Volumetric	
AKA - MSCT or Multislice CT	
Uses Helical/Spiral or Cone beam technology.	
Single breath hold capabilities.	

Image Formation	
CT System Principles, Operation, and Components	
Imaging Parameters and Data Acquisition	
Imaging Processing	
• 1. Reconstruction	
Filtered back projection	
Iterative reconstruction	· · · · · · · · · · · · · · · · · · ·
• Interpolation	
Reconstruction algorithm	
Raw data versus image data	
Prospective/retrospective reconstructive	
Reconstruction	-
Reconstruction thickness	
Reconstruction interval	
• 2. Post-Processing	
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Image Formation:	
Imaging Processing - Reconstruction	
An advancement of the Back-Projection method	
Summary of multiple projections to produce an image	
Does not produce a sharp image of the object and therefore is not used in	
the clinical CT	
	-
Filtered back projection	
Also known as the convoluted method	
The projection profile is filtered or convoluted to remove the blurring	
found in simple back projection techniques	
Commonly used in CT systems today	
54.	
nert	
USI (
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© 2018 OSKI_GINIOUSIS 41	
Image Formation:	
Imaging Processing - Reconstruction	
5 5 ·-··	
• Itorotivo vocenstvustion	
Iterative reconstruction	
Starts with an assumption and compares this assumption with measured	
values, makes corrections to bring the two into agreement, and then	
repeats this process over and over until the assumed and measured	
values are the same or within acceptable limits".	
Iterative algorithms consist of three steps	
• Input	
• IR Loop	
• Output	
Output	
nerl	
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	-
Image Formation: Imaging Processing - Reconstruction	
 Examples of Iterative Reconstruction Algorithms GE Healthcare: 	_
 Adaptive Statistical Iterative Reconstruction (ASIR) Veo Model-based Iterative Reconstruction Veo (MBIR) 	
Siemens: Image Reconstruction in Image Space (IRIS)	
Sinogram-Affirmed Image Reconstruction (SAFIRE) Philips:	
iDose (iterative processing in projection and image domains (iDOSE) Toshiba:	
Adaptive Iterative Dose Reduction (AIDR)	
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]
Image Formation: Imaging Processing - Reconstruction	
• Interpolation	
Reconstructs the spirally acquired images into what looks like individual slices	
 Two types 1. 360-degree linear interpolation	
• 2. 180-degree linear interpolation –The most common type.	
- 4	
<u>osrt</u>	
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Image Formation:	
Imaging Processing - Reconstruction	
Reconstruction algorithm – Filters!	
Bone Standard	
• Sharp	_
Smooth Edge	
• Lung	
ŌSTU	
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Image Formation:	
Imaging Processing - Reconstruction	
 Raw data versus image data Raw data is the result of preprocessed scan data that are subjected to the image 	-
reconstruction algorithm used by the scanner!	
LOSTI	
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Image Formation:	
Imaging Processing - Reconstruction	
Prospective/retrospective reconstruction	
 Prospective Reconstruction is done as the scan is acquired. Retrospective Construction is done after the scan has been acquired. 	
<u>~1.</u>	
OSTU	
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Image Formation: Imaging Processing - Reconstruction	
imaging Processing - Neconstruction	
Reconstruction thickness	
Slice thickness Slice thickness is an imaging parameter selected by the operator used	
 Slice thickness is an imaging parameter selected by the operator used in CT to define a dimension of depth adapted to the area of interest. 	
	-
<u>nort</u>	
OJIC	
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Image Formation:	
Imaging Processing - Reconstruction	
 Reconstruction interval Slice spacing or interval is determined by collimator spacing in a single array of detectors, further determined by the number and size of the detector elements grouped into each data channel. 	
<u>, </u>	
Tooth	
0 2018 OSAT, Galeouis 49	
Image Formation:	
Imaging Processing – Post Processing	
2. Post-Processing Multi-planar reformation (MPR) 3D rendering 9MIP, SSD, VR) Quantitative analysis (e.g., distance, diameter, calcium scoring, ejection	
fraction)	
<u> </u>	-
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Image Formation: Imaging Processing – Post Processing	
Multi-planar reformation (MPR)	
A method of altering the data that places the data in an different plane. CT is scanned in	
the axial plane; with only a few exceptions. But there may be a need to visualize the anatomy in another plane.	
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<u>osrt</u>	
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Image Formation:	
Imaging Processing – Post Processing	5

- 3D rendering (MIP, SSD, VR)
 - Methods of altering the data collected by the CT scanner in an different representation. CT has the capability of collecting massive amounts of data. These software adaptations allow for better visualization of the anatomy or pathology in question.



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Image Formation: Imaging Processing – Post Processing

- Quantitative analysis (e.g., distance, diameter, calcium scoring, ejection fraction)
 - QCT is a type of Computed Tomography that calculates and displays bone density in three dimensions.



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Image Evaluation and Archiving

- Image Display
 1. pixel, voxel
 2. matrix

 - 3. image magnification4. display field of view

 - 5. window level, window width
 - 6. cine
 - 7. geometric distance or region of interest (ROI) (e.g., mean, standard deviation [SD])

Image Evaluation and Archiving: Image Display • Pixel • Pixel = Picture element FOV • The formula used to discover pixel size is: • FOV/Matrix x FOV/Matrix = pixel size mm² • The larger the matrix, the smaller the pixel size Matrix e.g. 512 x 512 has a pixel size that is — and 256 x 256 has a pixel size that is ----*Smaller pixels will give you better spatial resolution!

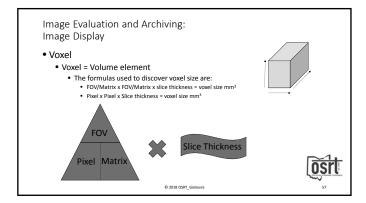


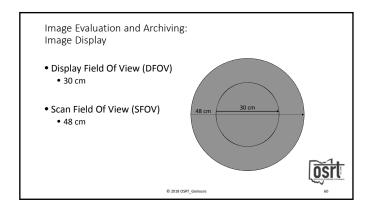
Image Evaluation and Archiving: Image Display	-
Matrix A series of columns and rows made up of pixels.	
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	-

Image Evaluation and Archiving: Image Display

- Image magnification
 - The enlargement of an image or a region of an image where the pixel size does not change.
 - Disadvantage image blur, distortion



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		_
Image Evaluation and Archiving: Image Display		
image Display		
 Attenuation – CT Numbers Tissue controls the rate of attenuation 		
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© 2018 OMT_Galouss	61	J
Imaga Figuration and Archiving		1
Image Evaluation and Archiving: Image Display		
 Attenuation – CT Numbers – aka Hounsfield numbers Window Width – Image Contrast 		
Window Level – Image Brightness		
	D4.	
	osrt	-
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Image Evaluation and Archiving: Image Display		
Window Level and Window Width		
Window Width		
WW on Image Contrast As the WW increases, the contrast decreases		
As the WW decreases, the contrast increasesContrast is optimized with medium WW settings		
Window Level	<u> </u>	
WL on Image Brightness	OSTU	
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Income Fuel cetion and Austriains		
Image Evaluation and Archiving: Image Display		
• Cine		
 Viewing images in a movie-like fashion. Overlapping thin image sets are used 		
 Pro - Increased spatial resolution 		
Con – Increased dose to the patient		
	nert	
	(USI t	
© 2018 OSRT_Gialousis	64	
Image Evaluation and Archiving:		
Image Display		
0		
 Geometric distance or region of interest (ROI) (e.g., mean, standard deviation [SD]) 		
Measurement tools to evaluate size or content of an anatomical		
structure or pathology.		
	nerl	
	(0316	
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Image Evaluation and Archiving		
Image Display		
Image Quality		
• 1. Spatial Resolution		
2. Contrast Resolution3. Temporal Resolution		
4. noise and Uniformity		
 5. Quality Assurance and Accreditation 		
6. CT Number (Hounsfield Units)7. Linearity	_	
Artifact Reconstruction and Reduction	osrt	
Informatics	0016	
© 2018 OSRT_Gialouxis	66	

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Image Evaluation and Archiving: Image Quality	
inage quarty	
 Spatial Resolution The ability to resolve closely placed objects that are significantly different from their background. 	
umerent nom then background.	
nert.	
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Image Evaluation and Archiving:	٦
Image Quality	-
 Contrast Resolution Is the ability to differentiate a structure that varies only slightly in density from its surroundings. 	
System sensitivity	
Low-contrast sensitivity	
nert.	
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	-
	٦
Image Evaluation and Archiving: Image Quality	
Temporal Resolution	
 An indication of a CT system's ability to freeze motions of a scanned object; performance parameter that deals in time or speed of data acquisition. 	
Important parameter when you want to minimize motion.	
lost	
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Image Evaluation and Archiving:	
Image Quality	
Noise and Uniformity	
 Noise – a random variation in CT numbers caused by attenuation of the x-ray beam as it passes through the anatomy of interest. Noise may also 	
be caused by disturbances that interfere with the normal flow of data	
through pathways of computers and other electrical devices.	-
Uniformity – the condition of being equal across all areas of a same	
tissue sample. For example, when you are doing a water phantom for QC and you take sample measurements at the center and along the	·
periphery of the phantom all measurements will be within a set	
variance to be considered normal.	-
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Image Evaluation and Archiving:	
Image Quality	
Quality Assurance and CT Accreditation (ACR)	
 QA is a program of Quality Control tests that periodically evaluate the performance of specific equipment. In this case CT equipment. 	
 There is a specific list of tests for CT equipment. This list displays the frequency 	
of each test and the normal variance permitted. The 3 principles of a good QA program are;	
Regular performance of QC tests to insure accurate results	
 Prompt interpretation of results Documented results with documentation of correction – if needed. 	
Accreditation is a voluntary program that demonstrates to patients and personnel of the CT facility the safety and effectiveness of their C1	
imaging services.	
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Image Evaluation and Archiving:	
Image Quality	
CT Number (Hounsfield Units)	
 CT numbers are based on the attenuation of x-rays through a particular type of tissue. 	
Hounsfield units are CT numbers!	
 Godfrey Hounsfield created the numbered system to represent the attenuation energy received by the IR as x-ray passed through a particular tissue. 	
 The first range was -500 for air, 0 for water, and +500 for bone. This was later changed to -1000 for air, 0 for water, and +1000 for bone – this is 	
what we use today!	
nort	
<u> </u>	
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		<u>-</u>
Image Evaluation and Archiving: Image Quality		
age Quanty		
• Linearity refers to the linear relationship of CT numbers in linear attenuation coefficients of the object to be imaged	to the d.	
		-
	ocri	
© 2018 OSRT_Gialousis	73	
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Image Evaluation and Archiving		
Artifact Recognition and Reduction 1. Beam hardening or cupping 2. Partial volume averaging		
3. Motion 4. Metallic 5. Edge gradient		
6. Patient positioning (out-of-field)7. Equipment induced		
RingsStreaksTube arc	<u>~1.</u>	
Cone beam Capping Information	osrl	
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		1
Sources of Image Artifact		
• The patient		
The maging process Equipment problems		
Malfunctions Imperfections		
Technologist error		
	<u>osrl</u>	
© 2018 OSRT_Glatowis	American Languages	

Beam-Hardening Artifact

- Appearance
 - Dark bands or streaks
 - Cupping at the center of the image
- Cause
 - Object size increases, low energy photons attenuated
 - Radiation beams have different path lengths
- Correction
 - Filter
 - Software



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Image Evaluation and Archiving: Artifact Recognition and Reduction

• Beam hardening or cupping



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Partial Volume Artifact

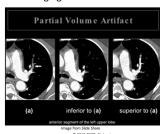
- Appearance
 - CT number representing an object is false
- Cause
 - Object is not fully within a slice thickness
 - Multiple objects in a slice
 - CT number is an average of all tissue types within the slice
- Correction
 - Thinner slices
 - Computer algorithms



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Image Evaluation and Archiving: Artifact Recognition and Reduction

• Partial volume averaging





Motion Artifact

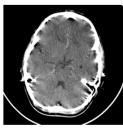
- Appearance
 - Streaks
- Cause
- Inability of reconstruction algorithm to account for inconsistencies
- Correction
 - Immobilize patient
 Short scan times

 - Software



Image Evaluation and Archiving: Artifact Recognition and Reduction

Motion



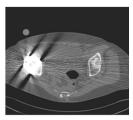


- Appearance
 - Streak and star-shaped artifact
- Cause
- Metallic object absorbs radiation, resulting in an incomplete projection profile
- Correction
 - Remove all metallic objects
 - Software



Image Evaluation and Archiving: Artifact Recognition and Reduction

Metallic





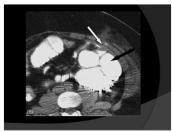
Edge Gradient Effect

- Appearance
 - Streaks
- Cause
 - Imaging an object that with an irregular shape or with a great difference in density
 Inconsistent attenuation information
- Correction
 - When applicable, over sample data beyond 360°
 - Thinner slices



Image Evaluation and Archiving: Artifact Recognition and Reduction

• Edge gradient





Out-of-field Artifact

- Appearance
 - Shading or streaking
- Cause
 - Anatomy out of the scan field of view contributes toward the attenuation and hardening of the x-ray beam
- Correction
 - Ensure all anatomy is contained within SFOV
 - Increase SFOV if possible



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Image Evaluation and Archiving: Artifact Recognition and Reduction

• Patient positioning (out-of-field)





Image Evaluation and Archiving:		
Artifact Recognition and Reduction • Equipment induced		
• Rings		
• Streaks		
Tube arc Cone beam		
• Capping		
	54.	
	osrl	
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		_
Image Evaluation and Archiving:		
Artifact Recognition and Reduction		-
• Rings		
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	(<u>USI</u>	
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Image Evaluation and Archiving: Artifact Recognition and Reduction		
Streaks		
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		<u> </u>

Image Evaluation and Archiving: Artifact Recognition and Reduction • Tube arc Image is from the Indian Journal of Radiology and Imaging © 2018 OSHT, Galousis	
Image Evaluation and Archiving: Artifact Recognition and Reduction • Cone beam Obtained from https://www.google.com/url/sa=i8rct=j&q=&esrc=s&source=images&cd=&cad=rja&uact=&evd=2ahUKEw jPgrWP6OfaAhVLGYMKHXKFBJsQjB16BAgBEAQ&url=https%3A%2P%2Evwww.auntminnie.com%2Eindex.aspx %3Fsec%30log%26itemiD%3D76261&psig=A0vVaw3Ww8W0CWChen2REmotf*Q3vt&ust=1525377448706539	
Image Evaluation and Archiving: Artifact Recognition and Reduction • Capping Output Output	

Image Evaluation and Archiving	_
image Quality Artifact Reconstruction and Reduction	
 Informatics 1. Hard/Electronic Copy (e.g., DICOM file format) 	
2. Archive3. PACS and electronic medical record (EMR)	
4. Security and confidentiality 5. Networking	
- J. Networking	
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Image Evaluation and Archiving: Informatics	
 Hard/Electronic Copy (e.g., DICOM file format) 	
 Imaging facilities have large servers that store an electronic copy of all exams performed at that facility. 	
DICOM is a special storage and sending format.DICOM	
D – DigitalI – Imaging and	
 CO – Communications in M - Medicine 	
n <u>ort</u>	
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Image Evaluation and Archiving:	
Informatics • Archive	
• Images are stored temporarily on the machine that acquired them.	-
 Images are then archived more permanently on CD's, DVD-R's, and in the cloud. 	
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Image Evaluation and Archiving:	
Informatics	
 PACS and electronic medical record (EMR) 	
• PACS	
• P – Picture	
• A – Archiving and	
C – CommunicationS – System	
• EMR	
 This is a secure medical record stored electronically of the patients health information. 	
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e la company de la company	
Image Evaluation and Archiving:	-
Informatics	
Security and confidentiality	
• HIPAA	
• H – Health	
 I – Insurance P – Portability and 	
• A – Accountability	
• A – Act	
HIPAA (Health Insurance Portability and Accountability Act of 1996) is United	
States legislation that provides data privacy and security provisions for safeguarding medical information.	
Surgest and meaner mornation	II C
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Income European and Aughbrine	
Image Evaluation and Archiving: Informatics	
• Networking	
Network topologies	
Local Area Network – LAN	
Metropolitan Area Network – MAN	
Wide Area network - WAN	
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